Biolimus-eluting versus everolimus-eluting stents in coronary artery disease: a pooled analysis from the NEXT (NOBORI biolimus-eluting versus XIENCE/PROMUS everolimus-eluting stent) and COMPARE II (Abluminal biodegradable polymer biolimus-eluting stent versus durable polymer everolimuseluting stent) randomised trials



**Georgios J. Vlachojannis**<sup>1</sup>, MD, PhD; Serban Puricel<sup>2</sup>, MD; Masahiro Natsuaki<sup>3</sup>, MD; Takeshi Morimoto<sup>4</sup>, MD, PhD, MPH; Pieter C. Smits<sup>1</sup>\*, MD, PhD; Takeshi Kimura<sup>5</sup>, MD; on behalf of the NEXT and COMPARE II investigators

1. Division of Cardiology, Maasstad Hospital, Rotterdam, The Netherlands; 2. Division of Cardiology, University of Fribourg, Fribourg, Switzerland; 3. Division of Cardiology, Saiseikai Fukuoka General Hospital, Fukuoka, Japan; 4. Department of Clinical Epidemiology, Hyogo College of Medicine, Nishinomiya, Japan; 5. Department of Cardiovascular Medicine, Kyoto University Graduate School of Medicine, Kyoto, Japan

G. J. Vlachojannis and S. Puricel contributed equally to this manuscript.

# KEYWORDS

- biodegradable polymer
- biolimus-eluting stent
- everolimus-eluting stent
- Nobori
- pooled analysis
- XIENCE

# Abstract

**Aims:** This study sought to investigate the safety and efficacy of a biolimus-eluting stent with biodegradable polymer (BP-BES) (Nobori; Terumo Corp.) compared to an everolimus-eluting stent with durable polymer (DP-EES) (XIENCE V or Prime; Abbott Vascular, or PROMUS; Boston Scientific).

**Methods and results:** The all-comers NEXT and COMPARE II clinical trials randomly assigned 5,942 patients to BP-BES (N=3,412) or DP-EES (N=2,530). We conducted a patient level pooled analysis at three-year follow-up with specified study endpoints: definite stent thrombosis (ST), the combined safety endpoint cardiac death or target vessel myocardial infarction (TV-MI), and the efficacy endpoint target lesion revascularisation (TLR). At three-year follow-up, all endpoints, namely definite stent thrombosis (BP-BES 0.8% vs. 0.4%, p=0.20), death or TV-MI (BP-BES 7.8% vs. 6.7%, p=0.07), as well as TLR (BP-BES 6.4% vs. 6.4%, p=0.78) were similar between groups. Interestingly, unadjusted (BP-BES 5.6% vs. 4.5%, p=0.02) and adjusted (HR 1.36; 1.01-1.82, p=0.04) TV-MI rates were higher in the BP-BES group than in the DP-EES group.

**Conclusions:** In this large-scale patient level pooled analysis of the NEXT and COMPARE II randomised trials, the use of BP-BES compared with DP-EES resulted in similar outcomes, but with an observed higher rate of TV-MI in the BP-BES group.

\*Corresponding author: Division of Cardiology, Maasstad Hospital, Maasstadweg 21, 3079 DZ Rotterdam, The Netherlands. E-mail: smitsp@maasstadziekenhuis.nl

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# Abbreviations

ACS	acute coronary syndrome
BP-BES	biodegradable polymer biolimus-eluting stent
CABG	coronary artery bypass grafting
CD	clinically driven
CI	confidence interval
COPD	chronic obstructive pulmonary disease
CVA	cerebrovascular accident
DAPT	dual antiplatelet therapy
DOCE	device-oriented composite endpoint
DP-EES	durable polymer everolimus-eluting stent
HR	hazard ratio
ITT	intention to treat
LAD	left anterior descending artery
LCX	left circumflex
LMT	left main trunk
MI	myocardial infarction
NSTEMI	non-ST-elevation myocardial infarction
Р	p-value
PCI	percutaneous coronary intervention
POCE	patient-oriented composite endpoint
RCA	right coronary artery
RIND	reversible ischaemic neurological deficit
SD	standard deviation
STEMI	ST-elevation myocardial infarction
TIA	transient ischaemic attack
TLR	target lesion revascularisation
TVR	target vessel revascularisation

# Introduction

Late adverse events such as very late stent thrombosis and restenosis after treatment with first-generation drug-eluting stents (DES) have been linked to vascular inflammatory response at the implantation site<sup>1-4</sup>. It has been hypothesised that the durable polymer responsible for drug elution plays a central role in promoting inflammation, thereby resulting in delayed re-endothelialisation and neoatherosclerosis<sup>5-9</sup>.

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DES with biodegradable polymer have been developed to mitigate this dilemma by combining the best of both worlds, the early efficacy of DES and the late safety associated with BMS. Initial data from a randomised trial indicated a biodegradable polymer-based biolimus-eluting stent (BP-BES) to be non-inferior with lower rates of very late stent thrombosis compared to the first-generation sirolimus-eluting stent CYPHER Select<sup>®</sup> (Cordis, Johnson & Johnson, Warren, NJ, USA)<sup>10,11</sup>.

However, newer-generation DES using a durable polymer have also been designed to improve polymer biocompatibility. Currently, the cobalt-chromium or platinum-chromium everolimus-eluting stent with durable fluoropolymer (DP-EES) is regarded as the gold standard due to its safety and efficacy profile<sup>12</sup>. Subsequent randomised all-comers trials documented similar outcomes for BP-BES compared to DP-EES up to three years<sup>13-17</sup>. However, none of the randomised studies was individually powered to account for low frequency events such as stent thrombosis, death or myocardial infarction (MI). Additionally, potential benefits of BP-BES with regard to these low frequency events might emerge at later follow-up.

Therefore, we conducted the present pooled analysis of the long-term follow-up from the prospective multicentre NEXT and COMPARE II trials, which are the largest trials to date to compare BP-BES to second-generation DP-EES.

# Methods

We performed a patient level pooled analysis of the NEXT (NOBORI Biolimus-Eluting Versus XIENCE/PROMUS Everolimus-eluting Stent Trial; NCT01303640) and COMPARE II (Abluminal biodegradable polymer biolimus-eluting stent versus durable polymer everolimus-eluting stent; NCT 01233453) randomised, allcomers trials which are to date the largest studies comparing BES with biodegradable polymer (a 316L stainless steel stent with 120 µm strut thickness and with a biodegradable poly-lactic acid polymer eluting the drug Biolimus A9<sup>™</sup> [Nobori<sup>®</sup>; Terumo Corp., Tokyo, Japan]) to EES with durable polymer (a cobalt- or platinumchromium metallic stent with a strut thickness of 81 µm and with a durable fluoropolymer eluting the drug everolimus [XIENCE V® or XIENCE Prime®; Abbott Vascular, Santa Clara, CA, USA, or PROMUS™; Boston Scientific, Marlborough, MA, USA]). Primary results including detailed descriptions of study methodology of the individual trials have been published previously<sup>13,14</sup>. Both trials included an all-comers PCI population, applying the same endpoint definitions as well as similar pre-specified follow-up time points. **Table 1** shows the main characteristics of the trials.

# PROCEDURE

PCI was carried out according to standard techniques. Technical details such as predilation, use of adjunctive vessel and lesion modification via thrombectomy or rotational atherectomy and decision about stent post-dilatation were left to the discretion of the operator. All patients not being on dual antiplatelet therapy prior to the procedure received aspirin and an oral loading dose of clopidogrel 300-600 mg before the index procedure. During the procedure, unfractionated heparin (70-100 IU/kg) was given with additional boluses as needed to achieve the recommended activated clotting time of 250 sec or longer. Use of glycoprotein IIb/IIIa inhibitors was at the discretion of the operator in the COMPARE II trial, while glycoprotein IIb/IIIa inhibitors were not available in the NEXT trial. All patients were discharged with aspirin 100 mg once daily indefinitely as well as a thienopyridine (clopidogrel 75 mg, ticlopidine 200 mg or prasugrel 10 mg once daily), with the recommended minimal duration of dual antiplatelet therapy (DAPT) being three months in the NEXT and 12 months in the COMPARE II trial.

# ENDPOINTS AND DEFINITIONS

The primary study outcome was defined by the endpoints which were specified before analysis implementation in conformity with

Table 1	. Characteristic	s of included	trials.
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	NEXT	COMPARE II
Number of ITT patients	3,235	2,707
Randomisation BP-BES: DP-EES	1:1	2:1
Primary endpoint	Death or myocardial infarction (safety) Target lesion revascularisation (efficacy)	Cardiac death, myocardial infarction, or target vessel revascularisation
Inclusion criteria	All-comers	All-comers
Exclusion criteria (major)	None	None
Baseline characteristics		
Mean age, years	69.2±9.8	62.9±11.1
Male, %	77.2	74.4
ACS, %	16.1	57.9
Diabetes, %	45.9	21.7
Lesion and procedure characteristics	(N=4,069)	(N=3,965)
Lesion length, mm	19.4±13.0	17.3±10.2
Reference diameter, mm	2.6±0.6	2.9±0.5
B2/C lesions, %	82.4	63.5
Aspirin duration	Indefinite	Indefinite
Thienopyridine duration	At least 3 months recommended	12 months recommended
Angiographic follow-up	Yes (in a total of 528 patients at 8-12 months)	No
Values are mean±SD or %.		

the Academic Research Consortium, including (1) stent thrombosis ("definite" and "definite or probable"), (2) the combined safety endpoint of cardiac death or MI (not clearly attributable to a nontarget vessel), and (3) target lesion revascularisation (TLR) as an efficacy measure.

Furthermore, the device-oriented composite endpoint (DOCE) consisting of cardiac death, MI (not clearly attributable to a non-target vessel), or TLR as well as the patient-oriented composite endpoint (POCE) defined as all-cause mortality, any MI, or any repeat revascularisation, and the respective individual endpoints were analysed.

All deaths were considered cardiac unless an unequivocal noncardiac cause was established. MI and stent thrombosis were defined according to the Academic Research Consortium (ARC) definition<sup>18</sup>. TLR was defined as any repeat percutaneous intervention of the target lesion within the stent or within the 5 mm borders adjacent to the stent or bypass surgery of the target vessel performed for restenosis or other complication of the target lesion. Clinically driven revascularisation of any target lesion (or vessel) was defined by either (1) stenosis of 50% of the lesion (or vessel) diameter on the basis of quantitative coronary angiography in the presence of objective evidence of ischaemia from non-invasive or invasive testing or symptoms; or (2) stenosis of at least 70% of the diameter of the lesion (or vessel), irrespective of ischaemic signs or symptoms.

#### FOLLOW-UP AND DATA MANAGEMENT

Data were captured in an electronic data form. Follow-up was performed via outpatient visit or phone at 12 months and yearly thereafter; additional follow-up was conducted at one and six months in the COMPARE II trial. Reportable clinical events were adjudicated by an independent committee blinded to treatment allocation.

#### STATISTICAL ANALYSIS

Categorical variables are presented as number and percentage, and were compared with the chi-square or Fisher's exact test. Continuous variables were expressed as mean±SD or medians with interquartile ranges. Normality was assessed by the visual inspection of QQ-plots and by the Shapiro-Wilk test. Continuous variables were compared using the Student's t-test or Wilcoxon rank-sum test based on their distribution. Both pooled studies were designed as randomised, non-inferiority all-comers trials. Because of the similarity between the two trials with regard to study design and endpoint definitions as well as follow-up times, we performed a simple data pooling. All analysis was performed according to the intention-to-treat principle. Cox proportional hazards regression stratified by trial was used for survival analysis. Nonviolation of the proportional hazards assumption was assessed on the basis of Schoenfeld's residuals. To assess heterogeneity across trials, we calculated Q-statistics. A two-sided alpha level of <0.05 was considered statistically significant. All Kaplan-Meier failure functions are provided in a non-stratified, non-adjusted manner. Statistical analyses were performed using Stata/MP 13 (StataCorp LP, College Station, TX, USA).

### Results

A total of 5,942 patients undergoing PCI were randomised to BP-BES (3,412 patients with 4,697 treated lesions) vs. DP-EES (2,530 patients with 3,397 treated lesions). Patient contribution from each trial as well as the key trial characteristics are shown in **Table 1.** Due to differences in baseline characteristics between the two trials coupled with the 2:1 (BP-BES:DP-EES) randomisation in the COMPARE II trial, significant baseline imbalances between treatment groups were observed after data pooling (**Table 2**). Briefly, patients treated with DP-EES were older and more often had diabetes and hypertension. On the other hand, patients treated with BP-BES more often presented with NSTEMI or STEMI.

Three-year clinical event rates are detailed in **Table 3** and **Figure 1**. Rates of definite stent thrombosis (BP-BES 0.8% vs. 0.4%, HR 1.71, and 95% CI: 0.76-3.88, p=0.20) as well as the combined safety endpoint of death or MI (BP-BES 7.8% vs. 6.7%, and HR 1.22, 95% CI: 0.99-1.54, p=0.07) were numerically higher in the BP-BES compared to the DP-EES group without reaching a statistically significant difference. The efficacy endpoint TLR as well as device and patient-oriented composite endpoints were similar between groups (**Table 3**).

Interestingly, a significant increase in the occurrence of MI in the BP-BES group was observed (BP-BES 6.5% vs. DP-EES

	BP-BES N=3,412	DP-EES N=2,530	<i>p</i> -value	
Age (years)	65.9±10.9	66.9±10.8	<0.01	
Male gender	75.6 (2,581)	76.3 (1,931)	0.56	
Diabetes	33.3 (1,136)	37.0 (937)	<0.01	
Hypertension	67.4 (2,300)	72.6 (1,836)	<0.01	
Current smoker	25.0 (854/3,411)	21.5 (543)	<0.01	
Previous smoker	36.7 (1,253/3,411)	37.4 (946)	0.61	
Never smoked	38.2 (1,304/3,411)	41.2 (1,041)	0.02	
Liver insufficiency	0.5 (18/3,394)	0.6 (14/2,519)	1.0	
Dialysis treatment	3.2 (109/3,392)	3.5 (87/2,519)	0.61	
COPD	5.2 (177/3,396)	4.3 (108/2,519)	0.11	
Previous stroke (CVA/TIA/RIND)	7.6 (260/3,409)	9.0 (228/2,528)	0.06	
Peripheral vascular disease	9.7 (156/1,617)	11.4 (185/1,618)	0.11	
Previous myocardial infarction	24.2 (822/3,402)	24.7 (624/2,524)	0.62	
Previous PTCA	33.3 (1,136)	38.5 (975)	<0.01	
Previous CABG	5.6 (190)	5.1 (129)	0.45	
Clinical presentation				
Stable angina	51.4 (1,754)	56.8 (1,436)	<0.01	
Silent ischaemia	10.2 (349)	12. 5 (315)	0.01	
Unstable angina	11.2 (382)	10.6 (268)	0.48	
NSTEMI	14.7 (503)	10.5 (265)	< 0.01	
STEMI	12.4 (424)	9.7 (246)	<0.01	
Values are mean±SD or %.				

#### Table 2. Baseline clinical characteristics.

5.3%, HR 1.35, CI: 1.04-1.75, p=0.03), which was driven by higher rates of target vessel MI (BP-BES 5.6% vs. DP-EES 4.5%, HR 1.41, CI: 1.05-1.89, p=0.02). The observed difference in target vessel MI is attenuated after adjustment for baseline imbalances but remains statistically significant (Table 4). There were no significant differences in treatment effects within any of the specified subgroups for the three main study outcomes or the DOCE, nor was any significant subgroup-treatment interaction found (data not shown).

No significant difference was observed regarding DAPT discontinuation between groups over the period of three years (Figure 2, Table 5). About 20% of patients had interrupted DAPT before 12 months and about 2.5% before six months without any occurrence of stent thrombosis (data not shown).

# Discussion

The principal finding of this large-scale pooled analysis is that the rates of specified safety and efficacy endpoints were similar between groups, apart from target vessel myocardial infarction which occurred more often in the BP-BES group.

Network meta-analyses have indicated an excess risk of biodegradable polymer drug-eluting stents with regard to MI or stent thrombosis when compared to DP-EES, though these analyses were restricted due to limited follow-up duration<sup>19-21</sup>. Of note, while the meta-analyses by Kang et al and Navarese et al included BP-BES trials using the BioMatrix<sup>TM</sup> device (Biosensors Europe SA, Morges, Switzerland) which is similar to the Nobori stent, the meta-analysis of Bangalore et al also included trials using a sirolimus-eluting stent with biodegradable polymer (Yukon<sup>®</sup> Choice PC; Translumina GmbH, Hechingen, Germany).

		BP-BES N=3,412	DP-EES N=2,530	HR (95% CI) (BP-BES/DP-EES)	<i>p</i> -value
Death	Any, n (%)	198 (5.8)	149 (5.9)	1.06 (0.85-1.32)	0.60
	Cardiac, n (%)	95 (2.8)	61 (2.4)	1.17 (0.84-1.62)	0.44
Myocardial	Any, n (%)	220 (6.5)	133 (5.3)	1.35 (1.04-1.75)	0.03
infarction	Target vessel MI, n (%)	190 (5.6)	113 (4.5)	1.41 (1.05-1.89)	0.02
Revascularisation	Any, n (%)	479 (14.0)	369 (14.6)	1.12 (0.97-1.28)	0.12
	Any TVR, n (%)	314 (9.2)	214 (8.5)	1.16 (0.97-1.39)	0.10
	Clinically driven TVR, n (%)	240 (7.0)	172 (6.8)	1.08 (0.88-1.32)	0.45
	Any TLR, n (%)	217 (6.4)	162 (6.4)	1.03 (0.84-1.27)	0.78
	Clinically driven TLR, n (%)	165 (4.8)	122 (4.8)	1.03 (0.81-1.31)	0.82
Stent thrombosis	Definite, n (%)	26 (0.8)	11 (0.4)	1.71 (0.76-3.88)	0.20
	Early, n (%)	13 (0.4)	4 (0.2)	2.83 (0.60-13.27)	0.19
	Late, n (%)	4 (0.1)	1 (0.0)	2.76 (0.30-25.16)	0.37
	Very late, n (%)	9 (0.3)	6 (0.2)	0.92 (0.32-2.62)	0.88
	Definite or probable, n (%)	28 (0.8)	17 (0.7)	1.17 (0.61-2.23)	0.64
Composite	Cardiac death or target vessel MI, n (%)	267 (7.8)	170 (6.7)	1.22 (0.99-1.54)	0.07
endpoints	DOCE, n (%)	430 (12.6)	301 (11.9)	1.20 (0.76-1.88)	0.12
	POCE, n (%)	755 (22.1)	579 (22.9)	1.09 (0.97-1.22)	0.15
Rates are reported as number (percentage). Hazard ratio provided as hazard BP-BES/hazard DP-EES and stratified according to trial (unadjusted).					

# Table 3. Unadjusted clinical outcomes at 3 years.



**Figure 1.** *Kaplan-Meier cumulative event curves. A) Target lesion revascularisation. B) Cardiac death or target vessel myocardial infarction. C) Target vessel myocardial infarction. D) Definite stent thrombosis.* 

		Adjusted for bas imbalance	seline s
		HR (95% CI)	<i>p</i> -value
Death	Any	1.05 (0.85-1.30)	0.66
	Cardiac	1.15 (0.82-1.60)	0.42
Myocardial	Any	1.05 (0.84-1.30)	0.68
infarction	Target vessel MI	1.36 (1.01-1.82)	0.04
Revascu-	Any	1.10 (0.96-1.26)	0.19
larisation	Any TVR	1.15 (0.96-1.37)	0.13
	Clinically driven TVR	1.06 (0.87-1.30)	0.54
	Any TLR	1.00 (0.82-1.24)	0.97
	Clinically driven TLR	1.01 (0.79-1.28)	0.95
Stent	Definite	1.45 (0.71-2.96)	0.30
thrombosis	Definite or probable	0.98 (0.53-1.79)	0.94
Composite endpoints	Cardiac death or target vessel MI	1.03 (0.84-1.25)	0.79
	DOCE	1.09 (0.96-1.27)	0.31
	POCE	1.07 (0.96-1.20)	0.24
Hazard ratio	provided as hazard BP-BES/ha	azard DP-EES.	

#### Table 4. Adjusted clinical outcome.



**Figure 2.** *Kaplan-Meier cumulative incidence of discontinuation of dual antiplatelet therapy.* 

However, the largest randomised all-comers trials, NEXT and COMPARE II, individually reported similar safety and efficacy results for the Nobori BP-BES compared to the second-generation DP-DES, namely DP-EES, at one and three years<sup>13,14,16,17</sup>. However, none of the individual trials was adequately powered for low frequency events such as stent thrombosis, death and MI.

	Interval	0 day	30 days	365 days	730 days	1,095 days
BP-BES group	No. of patients w/discontinuation		26	693	1,356	1,637
	No. of patients at risk	3,412	3,374	2,873	1,911	1,156
	Cumulative incidence		0.8%	20.3%	39.7%	48.0%
DP-EES group	No. of patients w/discontinuation		23	472	920	1,162
	No. of patients at risk	2,530	2,499	2,113	1,499	1,012
	Cumulative incidence		0.9%	18.7%	36.4%	45.9%

#### Table 5. DAPT discontinuation.

The present pooled analysis aimed to take these constraints into account, something which appears essential in the light of the attenuated power of the individual randomised studies due to lower than expected event rates of the primary endpoints used for sample-size calculation (almost 50% in the COMPARE II trial, about 30% in the NEXT trial).

Interestingly, while the present pooled analysis confirms results from the individual studies regarding similar efficacy outcomes, it indicates a significantly higher frequency of target vessel MI in the BP-BES group. This cannot be explained entirely through the numerically higher incidence of definite stent thrombosis in the BP-BES group. Thus, the pathophysiological mechanism triggering higher rates of target vessel MI remains partly unexplained. Drug and polymer properties, the stent platform design, material and, in particular, the strut thickness show significant differences between the tested devices which might lead to varying vascular healing responses. Indeed, strut thickness *per se* has been linked to higher rates of restenosis<sup>22,23</sup>.

Nevertheless, the benefit of biodegradable polymer-based stents is expected beyond one year. The LEADERS trial indicated lower very late stent thrombosis rates in patients treated with biodegradable polymer DES compared to the first-generation CYPHER DES<sup>10</sup>. However, the present analysis did not show benefits of the Nobori BP-BES at any of the analysed endpoints (including stent thrombosis) when compared to DP-EES. On the contrary, definite stent thrombosis occurred numerically more often in patients treated with BP-BES. Of note, the BP-BES cumulative definite stent thrombosis rate at three years was lower than the previously reported 1.4% in the SORT-OUT V trial<sup>17</sup>. Interestingly, we observed a very low definite stent thrombosis rate at three years in the DP-EES arm of 0.4%. Indeed, DP-EES possess an excellent safety profile when compared to other durable polymer DES and even BMS<sup>24</sup>. Finally, in both treatment arms no event of stent thrombosis was observed in patients who discontinued DAPT during the first 12 months after the index procedure.

By implication, the present results regarding the Nobori BP-BES cannot be generalised to other stent systems using biodegradable polymers, since the performance of these devices depends on interaction between the drug and its elution characteristics, the biodegradable polymer properties and the stent platform. Further data are warranted to indicate whether biodegradable polymer technologies with newer thin-strut stent platforms have added advantages in safety and efficacy when compared to current-generation thin-strut DES with durable polymer.

### Limitations

The study is limited by its *post hoc* nature; thus, the results should be considered hypothesis-generating. Furthermore, this analysis combined data from studies which enrolled patients from different ethnicities. Moreover, although each trial documented well balanced baseline characteristics, we observed significant baseline imbalances after pooling, which were accounted for via trial affiliation analysis and confirmed by multivariable adjusted hazard ratios which were very similar to the unadjusted hazard ratios.

### Conclusion

In this large-scale patient level pooled analysis from the NEXT and COMPARE II randomised trials, the use of Nobori BP-BES compared with DP-EES showed similar outcomes regarding the study specified endpoints but indicated a higher rate of target vesselrelated myocardial infarction with BP-BES at three years.

## Impact on daily practice

The present pooled analysis of the NEXT and COMPARE II trials shows that both the biodegradable polymer-coated biolimus-eluting stent (BP-BES) and the durable polymer-coated everolimus-eluting stents (DP-EES) have an excellent safety and efficacy profile for the specified endpoints, underlining the improved performance achieved with current-generation devices when compared to earlier-generation drug-eluting stents. Interestingly, the biodegradable polymer-coated BES does not indicate any benefit, in particular towards reduction of very late adverse events, and suggests higher rates of target vessel myocardial infarction, thus challenging the concept of biodegradable polymer coating in the tested setting.

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### **Conflict of interest statement**

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#### References

1. Finn AV, Kolodgie FD, Harnek J, Guerrero LJ, Acampado E, Tefera K, Skorija K, Weber DK, Gold HK, Virmani R. Differential response of delayed healing and persistent inflammation at sites of overlapping sirolimus- or paclitaxel-eluting stents. *Circulation*. 2005;112:270-8.

2. Hagiwara H, Hiraishi Y, Terao H, Hirai T, Sakaoka A, Sasaki M, Murota S, Inoue K, Kimura J. Vascular responses to a biodegradable polymer (polylactic acid) based biolimus A9-eluting stent in porcine models. *EuroIntervention*. 2012;8: 743-51.

3. Pendyala LK, Matsumoto D, Shinke T, Iwasaki T, Sugimoto R, Hou D, Chen JP, Singh J, King SB 3rd, Chronos N, Li J. Nobori stent shows less vascular inflammation and early recovery of endothelial function compared with Cypher stent. *JACC Cardiovasc Interv.* 2012;5:436-44.

4. Wilson GJ, Nakazawa G, Schwartz RS, Huibregtse B, Poff B, Herbst TJ, Baim DS, Virmani R. Comparison of inflammatory response after implantation of sirolimus- and paclitaxel-eluting stents in porcine coronary arteries. *Circulation*. 2009;120:141-9,1-2.

5. Byrne RA, Joner M, Kastrati A. Polymer coatings and delayed arterial healing following drug-eluting stent implantation. *Minerva Cardioangiol.* 2009;57:567-84.

6. Finn AV, Nakazawa G, Joner M, Kolodgie FD, Mont EK, Gold HK, Virmani R. Vascular responses to drug eluting stents: importance of delayed healing. *Arterioscler Thromb Vasc Biol.* 2007;27:1500-10.

7. Joner M, Finn AV, Farb A, Mont EK, Kolodgie FD, Ladich E, Kutys R, Skorija K, Gold HK, Virmani R. Pathology of drug-eluting stents in humans: delayed healing and late thrombotic risk. *J Am Coll Cardiol.* 2006;48:193-202.

8. Koppara T, Joner M, Bayer G, Steigerwald K, Diener T, Wittchow E. Histopathological comparison of biodegradable polymer and permanent polymer based sirolimus eluting stents in a porcine model of coronary stent implantation. *Thromb Haemost.* 2012;107:1161-71.

9. Nakazawa G, Finn AV, Joner M, Ladich E, Kutys R, Mont EK, Gold HK, Burke AP, Kolodgie FD, Virmani R. Delayed arterial healing and increased late stent thrombosis at culprit sites after drug-eluting stent placement for acute myocardial infarction patients: an autopsy study. *Circulation.* 2008;118:1138-45.

10. Serruys PW, Farooq V, Kalesan B, de Vries T, Buszman P, Linke A, Ischinger T, Klauss V, Eberli F, Wijns W, Morice MC, Di Mario C, Corti R, Antoni D, Sohn HY, Eerdmans P, Rademaker-Havinga T, van Es GA, Meier B, Jüni P, Windecker S. Improved safety and reduction in stent thrombosis associated with biodegradable polymer-based biolimus-eluting stents versus durable polymer-based sirolimus-eluting stents with coronary artery disease: final 5-year report of the LEADERS (Limus Eluted From A Durable Versus ERodable Stent Coating) randomized, noninferiority trial. *JACC Cardiovasc Interv.* 2013;6:777-89.

11. Windecker S, Serruys PW, Wandel S, Buszman P, Trznadel S, Linke A, Lenk K, Ischinger T, Klauss V, Eberli F, Corti R, Wijns W, Morice MC, di Mario C, Davies S, van Geuns RJ, Eerdmans P, van Es GA, Meier B, Jüni P. Biolimus-eluting stent with biodegradable polymer versus sirolimus-eluting stent with durable polymer for coronary revascularisation (LEADERS): a randomised non-inferiority trial. *Lancet.* 2008;372:1163-73.

12. Ormiston JA, Webster MW. Stent thrombosis: has the firestorm been extinguished? *Lancet*. 2012;379:1368-9.

13. Natsuaki M, Kozuma K, Morimoto T, Kadota K, Muramatsu T, Nakagawa Y, Akasaka T, Igarashi K, Tanabe K, Morino Y, Ishikawa T, Nishikawa H, Awata M, Abe M, Okada H, Takatsu Y, Ogata N, Kimura K, Urasawa K, Tarutani Y, Shiode N, Kimura T; NEXT Investigators. Biodegradable polymer biolimuseluting stent versus durable polymer everolimus-eluting stent: a randomized, controlled, noninferiority trial. *J Am Coll Cardiol.* 2013;62:181-90.

14. Smits PC, Hofma S, Togni M, Vazquez N, Valdes M, Voudris V, Slagboom T, Goy JJ, Vuillomenet A, Serra A, Nouche RT, den Heijer P, van der Ent M. Abluminal biodegradable polymer biolimus-eluting stent versus durable polymer everolimus-eluting stent (COMPARE II): a randomised, controlled, non-inferiority trial. *Lancet.* 2013;381:651-60.

15. Natsuaki M, Kozuma K, Morimoto T, Shiomi H, Kimura T. Two-year outcome of a randomized trial comparing second-generation drug-eluting stents using biodegradable or durable polymer. *JAMA*. 2014;311:2125-7.

16. Natsuaki M, Kozuma K, Morimoto T, Kadota K, Muramatsu T, Nakagawa Y, Akasaka T, Igarashi K, Tanabe K, Morino Y, Ishikawa T, Nishikawa H, Awata M, Abe M, Okada H, Takatsu Y, Ogata N, Kimura K, Urasawa K, Tarutani Y, Shiode N, Kimura T. Final 3-Year Outcome of a Randomized Trial Comparing Second-Generation Drug-Eluting Stents Using Either Biodegradable Polymer or Durable Polymer: NOBORI Biolimus-Eluting Versus XIENCE/PROMUS Everolimus-Eluting Stent Trial. *Circ Cardiovasc Interv.* 2015;8(10).

17. Vlachojannis GJ, Smits PC, Hofma SH, Togni M, Vazquez N, Valdes M, Voudris V, Puricel S, Slagboom T, Goy JJ, den Heijer P, van der Ent M. Long-term clinical outcomes of biodegradable polymer biolimus-eluting stents versus durable polymer everolimus-eluting stents in patients with coronary artery disease: three-year follow-up of the COMPARE II (Abluminal biodegradable polymer biolimus-eluting stent versus durable polymer everolimus-eluting stent) trial. *EuroIntervention*. 2015;11:272-9.

18. Cutlip DE, Windecker S, Mehran R, Boam A, Cohen DJ, van Es GA, Steg PG, Morel MA, Mauri L, Vranckx P, McFadden E, Lansky A, Hamon M, Krucoff MW, Serruys PW; Academic Research Consortium. Clinical end points in coronary stent trials: a case for standardized definitions. *Circulation*. 2007;115: 2344-51.

19. Kang SH, Park KW, Kang DY, Lim WH, Park KT, Han JK, Kang HJ, Koo BK, Oh BH, Park YB, Kandzari DE, Cohen DJ, Hwang SS, Kim HS. Biodegradable-polymer drug-eluting stents vs. bare metal stents vs. durable-polymer drug-eluting stents:

a systematic review and Bayesian approach network meta-analysis. *Eur Heart J.* 2014;35:1147-58.

20. Bangalore S, Hannan EL, Toklu B, Amoroso N, Fusaro M, Kumar S, Faxon DP, Feit F. Bare metal stents, durable polymer drug eluting stents, and biodegradable polymer drug eluting stents for coronary artery disease: mixed treatment comparison meta-analysis. *BMJ.* 2013;347:f6625.

21. Navarese EP, Tandjung K, Claessen B, Andreotti F, Kowalewski M, Kandzari DE, Kereiakes DJ, Waksman R, Mauri L, Meredith IT, Finn AV, Kim HS, Kubica J, Suryapranata H, Aprami TM, Di Pasquale G, von Birgelen C, Kedhi E. Safety and efficacy outcomes of first and second generation durable polymer drug eluting stents and biodegradable polymer biolimus eluting stents in clinical practice: comprehensive network meta-analysis. *BMJ.* 2013;347:f6530.

22. Kastrati A, Mehilli J, Dirschinger J, Dotzer F, Schuhlen H, Neumann FJ, Fleckenstein M, Pfafferott C, Seyfarth M, Schomig A. Intracoronary stenting and angiographic results: strut thickness effect on restenosis outcome (ISAR-STEREO) trial. *Circulation*. 2001;103:2816-21.

23. Pache J, Kastrati A, Mehilli J, Schuhlen H, Dotzer F, Hausleiter J, Fleckenstein M, Neumann FJ, Sattelberger U, Schmitt C, Muller M, Dirschinger J, Schomig A. Intracoronary stenting and angiographic results: strut thickness effect on restenosis outcome (ISAR-STEREO-2) trial. *J Am Coll Cardiol.* 2003;41:1283-8.

24. Palmerini T, Benedetto U, Biondi-Zoccai G, Della Riva D, Bacchi-Reggiani L, Smits PC, Vlachojannis GJ, Jensen LO, Christiansen EH, Berencsi K, Valgimigli M, Orlandi C, Petrou M, Rapezzi C, Stone GW. Long-Term Safety of Drug-Eluting and Bare-Metal Stents: Evidence From a Comprehensive Network Meta-Analysis. *J Am Coll Cardiol.* 2015;65:2496-507.